Accommodating IOL Designs

What elements are needed in accommodating IOL designs to make them successful?

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RST Europe asked an international panel of leading surgeons the following question: What elements are needed in accommodating IOL designs to make them successful? Their answers are below.

EDUARDO F. MARQUES, MD

Based on my experience, there are five essential elements in successful accommodating IOL designs, as outlined below.

No. 1: Allow spectacle independence for all distances. A successful accommodating IOL should provide enough pseudophakic accommodation to allow spectacle independence for all distances. This can be achieved using one or a combination of the two physiologic changes that also occur in the natural lens with contraction of the ciliary muscle:

- Increase in paraxial power of the IOL. This is the mechanism used in the Synchrony dual-optic accommodating IOL (Abbott Medical Optics), which changes the relative distance between the IOL's two optics with ciliary muscle contraction, thus increasing paraxial power and providing intermediate and near focus. This mechanism has been demonstrated objectively in patients up to 4 years after implantation of the IOL. It was also one of the mechanisms of action suggested for the Crystalens accommodating IOL (Bausch + Lomb), which is believed to move anteriorly with contraction of the ciliary body, although this is controversial.
- Increase in anterior curvature of the IOL. Some believe
 this is the mechanism of action of the Crystalens,
 which may change shape due to its flexible material.
 Additionally, the second generation of the dualoptic accommodating IOL (Synchrony Vu) includes
 a central area of negative spherical aberration on
 the surface of the anterior optic to try to mimic the
 changes occurring in the natural lens during ciliary
 body contraction. In theory, this change allows a
 gain of 1.00 D depth of focus for near.

No. 2: Guarantee the same optical quality as a monofocal IOL. The main advantage of accommodating

IOLs is the lower incidence of the dysphotopsia and loss of contrast sensitivity that are typical of multifocal IOLs. This is due to the use of monofocal optics, a trait that all available accommodating IOLs have in common.

No. 3: Afford excellent refractive predictability. One of the criticisms regarding existing accommodating IOLs is their lower refractive predictability compared with multifocal IOLs. Stability and final position of an accommodating IOL depends largely on the size and shape of the patient's capsular bag, as well as contraction and fibrosis of the bag, which interfere with the refractive result. The design of accommodating IOLs should provide good stability and adaptation to the bag, allowing precise IOL power calculation.

No. 4: Allow easy, safe implantation through a small incision. Small incisions induce less astigmatism, allow quicker recovery, and provide increased safety compared with larger incisions. One of the difficulties with accommodating IOLs has been the need for larger incisions to implant these more complex devices.

No. 5: Prevent posterior capsular opacification (PCO). Prevention of PCO is an essential characteristic of a successful IOL. The rate of PCO is lower with dual-optic IOLs than with single-optic, probably due to the maintenance of an open system, allowing circulation of aqueous in the capsular bag. Other strategies include the more common use of a square optic edge.

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PETER MOJZIS, MD

The development of accommodating IOLs to restore the dynamic dioptric range in presbyopic and cataract patients has been a challenge for many years. Accommodation in phakic patients

is achieved by one or a combination of some of the follow-

ing mechanisms: ciliary muscle movement, change of lens shape, and increased vitreous pressure. Unfortunately, artificial reproduction of the process of accommodation is a complex issue.

Different techniques have been used to develop accommodating IOLs, such as anterior movement and steepening of the anterior surface of the IOL as a result of ciliary muscle contraction (NuLens [NuLens]; FluidVision lens [PowerVision]) or anterior vaulting and axial movement of the IOL (Crystalens; Tetraflex [Lenstec]).

Another interesting concept is the replacement of the crystalline lens with a polymer material that, theoretically, acquires the lens shape after polymerization (SmartLens; Medennium). The main concerns with this approach are leakage of the polymer and the development of PCO.

I am convinced that the IOL design of the Light Adjustable Lens (Calhoun Vision) may be adequate to achieve an accommodative effect. This lens consists of a photosensitive silicone material that can be adjusted to the desired refractive power using ultraviolet (UV) light.

In my opinion, considering the mechanism of accommodation using only one concept to achieve artificial accommodation is insufficient. A promising new project is a lens that combines several mechanisms, the WIOL-CF (Medicem). The WIOL-CF is a polyfocal accommodating lens made of a special hydrogel material with properties comparable to those of the natural lens. The lens is flexible and soft and has a diameter of 8.9 mm, similar to the size of the crystalline lens. Its material enables the IOL position and shape to change during contraction or relaxation of the ciliary muscle.

The smooth surface and size of the WIOL-CF help to ensure perfect centration and stability and to prevent PCO formation. Another important feature is the polyfocality of this IOL, which is created by its hyperbolic curvature. Further, the additive effect of pseudoaccomodation facilitates near vision. This combination of three mechanisms of action—accommodation, pseudoaccomodation, and polyfocality—may be an approach that leads to a functional level of visual acuity at different distances. For this reason, I prefer the WIOL-CF.

The ideal accommodating IOL should provide emmetropia for distance, produce a sufficient amount of accommodative range with minimal aberrations during deformation, and be capable of injection through a microincision. The polymerization process should be safe and stable, without any adverse events. The ability to adjust IOL power and customize the lens postoperatively is desirable. The main benefit of this premium IOL should be its ability to generate a variable focus at any time depending on the patient's need.

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Suggested Reading List

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EWA MRUKWA-KOMINEK, MD, PHD

To determine the elements of successful accommodating IOL designs, we must first understand the mechanism of accommodation, which has been studied at least since the

time of Helmholtz. During cataract surgery, the natural crystalline lens is replaced with a prosthetic IOL with a fixed power to produce emmetropia. Because the natural lens changes power at different distances of focus, accommodating IOLs should also have the ability to change lens power. They should be designed to change the eye's power or focal length with the patient's natural efforts to accommodate.

The aim of accommodating lens development has been to mirror the properties of the natural crystalline lens as closely as possible. These elements can be divided into material, design, and function. The material of an accommodating IOL should enable it to change refractive power. The IOL should have a size close to that of the natural lens (10 mm), hydration close to 62% water content, and a refractive index close to 1.43. The lens should also have a smooth, highly hydrated surface; be resistant to protein adsorption and cell attachment; and have glare-free optics with an antireflective surface, a negative charge, and a material that absorbs UV light.

Currently, the accommodating IOL that is most similar to the natural lens is the WIOL-CF bioanalogic accommodating polyfocal lens. It has large, glare-free continuous hyperbolic aspheric optics and a full-disc plano-convex lens up to 9 mm. The full-disc configuration results in self-centration, excellent stability, resistance to dislocation, and optics with no zones, thus providing excellent contrast sensitivity. A continuous transition between the optics and rim yield no edge effects, improving night vision and minimizing glare.

The WIOL-CF's sharp-edged continuous rim and smooth, convex hyperbolic surface closely adhere to the posterior capsule and do not allow penetration of cells behind the lens, making the lens resistant to PCO. The aspheric hyperboloid optics improve its depth of focus. Water content of the WIOL-CF material is 42%, and the refractive index is 1.43, similar to that of the natural lens. Its low refractive index results in minimal surface reflection and glare at night. The lens is made of a highly biocompatible material and

has a smooth, negative-charged surface, which influences its resistance to proteins, cell attachment, and PCO and does not cause adhesion to tissue. Another important feature is the lens' ability to be injected through a small incision.

Pseudophakic accommodation may be a result of several different mechanisms. Near focus could primarily be due to lens deformation—a result of ciliary muscle contraction and vitreous body back-stop support—and far focus could be a result of lens polyfocality, anterior-to-posterior movement, and shape relaxation. Accommodating lens designs that take into account this combination of mechanisms may improve patients' overall visual results.

The WIOL-CF achieves its results through its unique design and material developed to resemble the properties of the natural crystalline lens. Implantation of the WIOL-CF restores many of the characteristics of the young natural crystalline lens in terms of its optics, function, and position in the eye. It provides the retina and brain with comprehensive and understandable visual information. Therefore, the WIOL-CF represents a leading technology for the treatment of cataract and presbyopia in patients who demand more than good visual acuity at selected, predefined distances.

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DOMINIQUE PIETRINI, MD

Truly accommodating IOLs are our greatest challenge in regard to presbyopia correction following cataract surgery. The accommodative effect of these IOLs depends on many factors, chiefly

the lens and optic designs.

First, researchers and manufacturers must consider the variability of the size of the capsular bag, which can range from 9 to 12 mm, according to Mana Therani, MD.¹ Most recently designed accommodating IOLs try to mimic the natural crystalline lens shape, and the relationship between the IOL and the capsular bag equator is the basis of reliable transmission of the forces applied to the bag by ciliary muscle action. This condition is crucial for all types of accommodating IOLs, based on displacement of the optic to obtain the maximum and optimal repeatable effect on optic movement. The IOL should have the ability to stay in contact with the equator in bags of all sizes or to be customized based on preopera-

tive evaluation of capsular bag size. The ideal volume of the lens should also be integrated into the design, especially for lens-refilling techniques.

Most accommodating IOLs based on optic displacement (single- and dual-optic lenses) are naturally unstable. The IOL design should consider postoperative changes in the conditions of the capsular bag, such as shrinkage and variable changes in the capsular response depending of the presence of residual lens epithelial cells (LECs). The presence of LECs leads to anterior capsular fibrosis, which may affect the accommodative response due to changes in capsular elasticity. The fibrous metaplasia of anterior LECs may improve lens fixation, but it may also lead to decentration of unstable optics. On the other hand, thorough cleaning of anterior LECs could lead to IOL instability and capsular thinning, as recently suggested by David J. Spalton, MD.²

Control of postoperative capsular opacification and fibrosis will improve the predictability and repeatability of the effect and open the field to lens-refilling techniques, including Phaco-Ersatz³ and the SmartLens. Large optics and small incisions are mandatory to achieve optimal results and good quality of vision.

The optic component also plays a major role in pseudoaccommodation. For single-optic IOLs including the Crystalens, 1CU (HumanOptics), and Tetraflex, the anterior displacement of the optic will never be sufficient to provide full accommodation; this mode also depends on the power of the lens, favoring higher lens powers. The optic must be improved for better effect, through inclusion of an aspheric component or the ability to change the central power with ciliary muscle action.

For dual-optic IOLs, this effect is theoretically more important, and evolution of the design, with better transmission of ciliary forces to the anterior optic, should improve performance.

Overall, restoration of accommodation is a field of ophthalmology in which research and investigation will bring improvements in our understanding of the accommodative process, and these will result in better-performing accommodating IOLs with new designs and concepts.

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